

BRAIN TUMOR DIAGNOSIS USING NANO DIGITAL TOPOLOGY

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ABSTRACT

In this paper, a Nano topological boundary approach is introduced for the identification of brain tumor in *digital images*.

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1. INTRODUCTION

Brain tumors, abnormal growths within the brain, pose a significant threat to human health. Early and accurate diagnosis is crucial for effective treatment and improved patient outcomes. Medical imaging techniques, particularly Magnetic Resonance Imaging (MRI), play a vital role in the detection and characterization of these tumors. However, the interpretation of MRI scans can be challenging due to the complexity of brain structures and the variability in tumor appearance. Digital image processing techniques offer powerful tools for analyzing medical images, aiding radiologists in the diagnostic process. This article explores the application of Nano Digital Topology (NDT) for the analysis of brain tumor images derived from MRI scans. NDT, a framework that combines concepts from digital topology and rough set theory, provides a robust approach for handling the inherent vagueness and uncertainty associated with digital representations of continuous objects, such as tumors in medical images.

Traditional digital topology often relies on precise definitions of connectivity and boundaries, which can be sensitive to noise and discretization artifacts. Rough set theory, on the other hand, deals with uncertainty by defining objects based on lower and upper approximations. By integrating these two approaches, NDT offers a more flexible and resilient framework for analyzing the topological properties of digital objects extracted from medical images. This article will delve into the methodology of applying NDT to brain tumor diagnosis using MRI images. It will discuss the key steps involved, including image preprocessing, segmentation, topological feature extraction using rough set principles, and potential classification strategies. The aim is to demonstrate how NDT can provide valuable insights into the structural characteristics of brain tumors, potentially improving diagnostic accuracy and reducing the rate of false positives and negatives.

2. PRELIMINARIES

Definition.2.1 [3]:

Two lattice points in the plane are said to be *8-adjacent* if they are distinct and each coordinate of one differs from the corresponding coordinate of the other by at most 1.

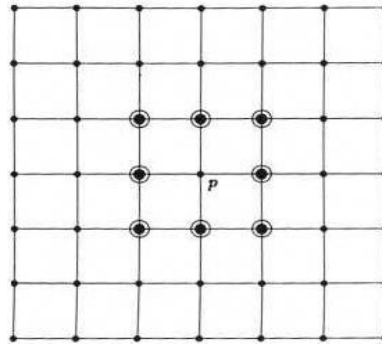


Fig.2.1

Definition.2.2 [3]:

Two lattice points in the plane are said to be **4-adjacent** if they are 8-adjacent and differ in at most one of their coordinates. That is any pixel $p(x,y)$ has two vertical and two horizontal neighbors, given by:

$$(x+1, y), (x-1, y), (x, y+1), (x, y-1)$$

Definition.2.3 [3]:

A lattice point associated with a pixel or voxel that has value 1 is called **black point** ($\bullet$). A lattice point associated with a pixel or voxel with value 0 is called a **white point** ($\circ$).

Definition.2.4 [3]:

A **digital picture** is a quadruple (V, m, n, B) , where $V = Z^2$, $B \subseteq V$ and where $(m, n) = (4, 8)$ or $(8, 4)$ if $V = Z^2$. The elements of V are called the points of the digital picture. The points in B are called the black points of the picture; the points in $V - B$ are called the white points of the picture.

Definition.2.5 [3]:

Two black points in a digital picture (V, m, n, B) are said to be **adjacent** if they are m-adjacent and two white points or a white point and a black point are said to be adjacent if they are n-adjacent. A Straight line segment that joins two adjacent points is called an adjacency.

Definition.2.6 [3]:

A **component** of a set of black and/or white points S is a non-empty connected subset of S which is not adjacent to any other point in S . In a (m, n) digital picture a component of a set of black points is an m-component, whereas a component of a set of white points is an n-component.

Definition.2.7 [3]:

A component of the set of all black points of a digital picture is called **black component**, and a component of the set of all white points is called a **white component**. In a finite digital picture there is a unique infinite white component, which is called the **background**.

Definition.2.8 [8]:

Let U be a certain set called the universe, and let R be an equivalence relation on U named as indiscernibility relation. The pair $A = (U, R)$ will be called an **approximation space**. If $x, y \in U$ and $(x, y) \in R$ we say that x and y are indistinguishable in A . Let $X \subseteq U$.

- (i). The lower approximation of a set X with respect to R is the set of all objects, which can be for certain classified as X with respect to R (are certainly X with respect to R) and its is denoted by $\underline{R}(X)$. That is, $\underline{R}(X) = \cup \{Y \in U / R : Y \subseteq X\}$.
- (ii). The upper approximation of a set X with respect to R is the set of all objects which can be possibly classified as X with respect to R (are possibly X in view of R) and it is denoted by $\overline{R}(X)$. That is $\overline{R}(X) = \cup \{Y \in U / R : Y \cap X \neq \emptyset\}$
- (iii). The boundary region of a set X with respect to R is the set of all objects, which can be classified neither as X nor as not- X with respect to R and it is denoted by $BN_R(X) = \overline{R}(X) - \underline{R}(X)$.

Definition.2.9 [8]:

Let U be a certain set called the universe, and let R be an equivalence relation on U named as indiscernibility relation. Let $X \subseteq U$.

- (i). A set X is crisp (exact with respect to R), if the boundary region of X is empty. That is $\overline{R}(X) = \underline{R}(X)$.
- (ii). A set X is rough (inexact with respect to R), if the boundary region of X is nonempty. That is $\overline{R}(X) \neq \underline{R}(X)$.

3. NANO DIGITAL IMAGE PROCESSING TECHNIQUES

This section outlines the proposed methodology for brain tumor diagnosis utilizing Nano Digital Topology. The brain tumor detection system implemented in this paper follows a five-step procedure. Input MRI images, sourced from radiology websites containing brain tumor cases. Following the acquisition of these MRI images, the initial preprocessing stage involves converting RGB images to grayscale and applying a thinning technique to enhance

the tumor region. Subsequently, the image is transformed into a (4,8) connected component digital representation. Nano approximation techniques are then applied to this digital image, and finally, the tumor is segmented within the Nano approximation space. This final segmentation step aims to achieve precise, edge-to-edge detection of the brain tumor. A comprehensive block diagram of this proposed system is presented in Figure 3.1, and the subsequent subsections provide a detailed discussion of each step.

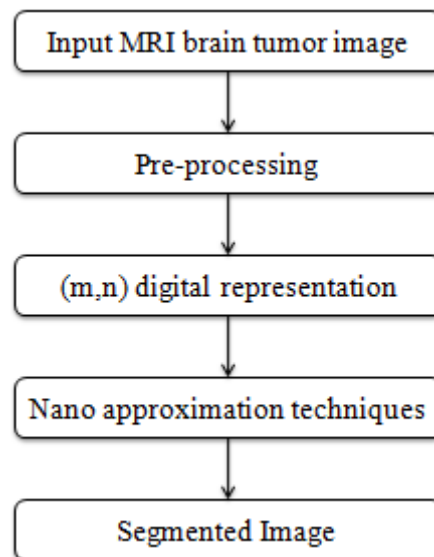


Figure.3.1

3.1. Input Image

The initial step in the proposed system is the acquisition of MRI brain tumor images. This work relies on MRI scans to diagnose brain tumors. MRI image acquisition retrieves images from a hardware source. MRI images are typically stored in a digital format (e.g., DICOM) to facilitate processing with image processing algorithms. Various MRI sequences, such as T1-weighted, T2-weighted, and FLAIR (Fluid-Attenuated Inversion Recovery), are often acquired, each providing different information about brain tissues. T2-weighted and FLAIR sequences are particularly important for brain tumor detection due to their sensitivity to edema and pathological changes. For the practical implementation within this research work, MRI images in common image formats such as JPG or PNG are utilized due to their ease of processing in standard image processing software and algorithms. Figure 3.2 illustrates a representative MRI image of the brain used in this research.

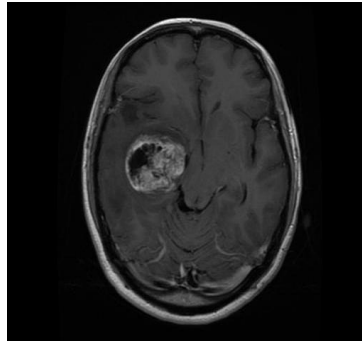


Figure 3.2. MRI Brain Tumor

3.2. Image Preprocessing

Preprocessing is an essential stage in the analysis of MRI brain tumor images, as it significantly influences the quality and suitability of the images for subsequent processing steps. MRI images often contain noise and other artifacts that can hinder accurate tumor detection, making preprocessing crucial for enhancing the visibility of relevant features. This section outlines the specific preprocessing procedures applied to the input MRI images. The preprocessing stage in this proposed system involves the following steps, as further illustrated in Figure 3.3:

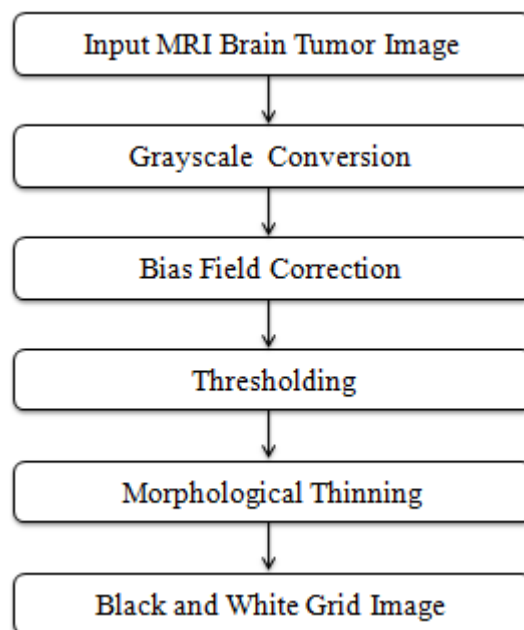


Figure.3.3

3.2.1. Grayscale Conversion

The input to the preprocessing stage is a digital MRI image of the brain. If the input MRI image is a color image, it is converted into a grayscale image. This conversion

simplifies the image data by reducing the number of color channels to one (intensity), which can improve processing efficiency and reduce computational complexity. Working with grayscale images is particularly advantageous for many image processing algorithms that are designed to operate on single-channel intensity information, rather than multi-channel color data. This step ensures uniformity in image representation across the dataset, which is critical for consistent application of subsequent analytical techniques, including bias field correction, thresholding, and the core Nano approximation methods. The intensity values in the grayscale image will directly correspond to the signal strength captured by the MRI scanner, making them suitable for distinguishing different tissue types and anomalies such as tumors based on their inherent signal characteristics.

3.2.2. Bias Field Correction

MRI images can suffer from intensity inhomogeneities, also known as bias fields, which are slow spatial variations in signal intensity across the image. These variations are typically caused by imperfections in the magnetic field and radiofrequency coil sensitivity. Bias field correction algorithms are applied to compensate for these variations and restore intensity uniformity across the image volume. This ensures that variations in pixel intensity accurately reflect intrinsic tissue differences (such as those between normal brain tissue and a tumor) rather than being artifacts of the scanning process. Effective bias field correction is critical for accurate quantitative analysis and reliable segmentation in medical images, as it standardizes the signal intensity distribution.

3.2.3. Thresholding

Thresholding is a fundamental image segmentation technique applied to the preprocessed grayscale image. Its primary purpose is to partition the image into distinct regions based on pixel intensity values, effectively converting a grayscale image into a binary one. In the context of brain tumor detection, pixels with intensity values above a certain empirically determined or adaptively calculated threshold are classified as belonging to a potential tumor region, while those below the threshold are classified as belonging to the background or normal brain tissue. This operation is computationally efficient and can provide a preliminary segmentation, highlighting areas of interest. However, it is important to note that global thresholding can be sensitive to intensity variations within the tumor itself or surrounding healthy tissue, making it a challenging step that often requires further refinement or more sophisticated techniques to define precise tumor boundaries.

3.2.4. Morphological Thinning

Following the thresholding operation, morphological thinning is applied. This image processing technique is used to reduce the thickness of binary objects (like the segmented tumor region or its boundaries) to a single pixel width, without altering the essential topological characteristics such as connectivity. The process iteratively removes pixels from the object's boundary while preserving end points and connectivity. Thinning can significantly simplify the representation of complex shapes, making subsequent analyses, particularly those involving digital topology and boundary feature extraction, more efficient and robust. For brain tumor analysis, thinning helps in obtaining a skeletonized representation of the tumor's boundary or internal structures, which can be valuable for shape analysis and for the identification of Nano boundary points.

3.2.5. Black and White Grid Image

The final step in the preprocessing stage involves transforming the refined image into a black and white grid representation. This conversion is crucial as it prepares the image for the application of Nano approximation techniques, which operate on binary digital pictures. In this representation, each pixel, now either black (representing a value of 1) or white (representing a value of 0), forms the fundamental unit of a digital grid. This binary format simplifies the image data to its most essential topological components, making it amenable to the precise definitions and operations of Nano digital topology. The black points typically correspond to the regions of interest, such as potential tumor areas, while the white points represent the background or surrounding healthy tissue, thereby setting the stage for the detailed analysis of connectivity and boundaries in the subsequent stages of the proposed system.

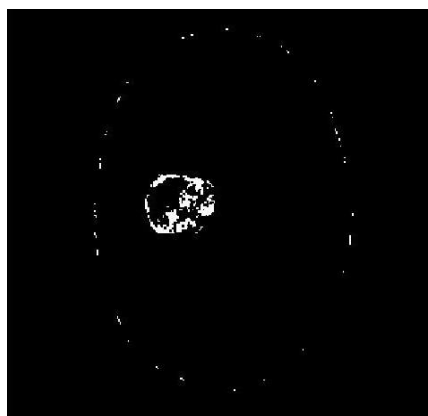


Figure 3.4. Black and White Grid Image

3.3. Digital Representation

Following the comprehensive preprocessing stage, the black and white grid image (the output of Section 3.2.5) is formally transformed into a digital picture, which serves as the foundational structure for applying Nano Digital Topology. This digital representation provides a discrete, topological framework of the brain MRI. By establishing the image as a formal digital picture, the system can rigorously apply the definitions of adjacency, connectivity, and components as outlined in the Preliminaries. This structured representation is indispensable for the subsequent application of Nano Approximation Techniques, as it allows for the precise calculation of lower and upper approximations and the identification of Nano topological boundaries, which are critical for accurate tumor segmentation.

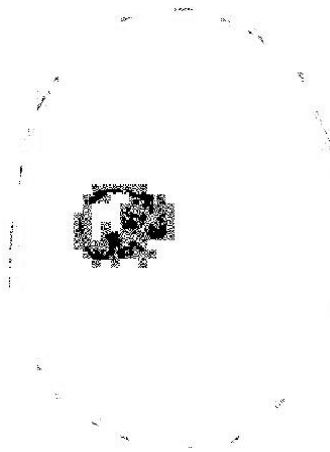


Figure 3.5. (m, n) Digital Representation

3.4. Nano Approximation Techniques

Rough set theory provides an approximation space whose topology is generated by equivalence classes derived from an indiscernibility relation. This partition defines an approximation space $A = (U, R)$, where U is a set called the universe (in this context, the set of all pixels in the digital image), and R is an equivalence relation that groups indistinguishable pixels. These equivalence classes are also known as granules, elementary sets, or blocks. Rough sets have proven successful in various image processing tasks, including segmentation, enhancement, and classification, particularly due to their ability to handle vagueness and uncertainty inherent in digital representations.

Figure 3.6 illustrates the fundamental concept of a rough set. For a given object X , the **lower approximation** ($\underline{N}(X)$) comprises all elementary sets (granules) that are *entirely included* within X . These elements are certainly members of X . The **upper approximation**

$(\bar{N}(X))$ consists of all elementary sets that have a *non-empty intersection* with X . These elements are possibly members of X . The region between the lower and upper approximations is the **boundary region** ($N_{BND}(X)$), representing elements that cannot be definitively classified as either belonging or not belonging to X . This mechanism offers a robust tool to deal with inconsistencies and imprecision.

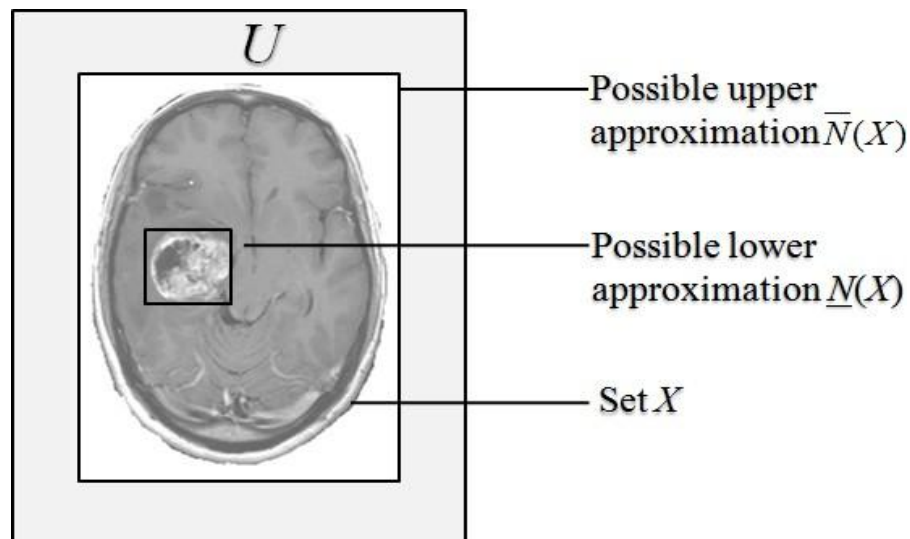


Figure 3.6. An Example Representation of a Nano Digital Topology

In the context of the digital MRI brain tumor image, which is now represented as a black and white grid (as described in Section 3.2.5), these nano approximation concepts are applied. If the set of all black points is considered as the potential tumor region (set X):

- The **lower approximation** of this set of black points (the potential tumor) would be composed of all elementary sets (pixel groups defined by the indiscernibility relation) that are *entirely black* and thus certainly belong to the tumor region.
- The **upper approximation** would be composed of all elementary sets that contain *at least one black point*, meaning they possibly belong to the tumor region.

A pixel is identified as a **Nano boundary point** if it is a black point adjacent to one or more white points. This definition is consistent with digital topology, where boundaries are often defined by adjacencies between a set and its complement. Pixels with intensity values above a certain threshold, classified as black points, form the potential tumor region (black component). In a finite digital picture, there is a unique infinite white component, which is referred to as the Nano background. The Nano boundary points effectively delineate the outline of the brain tumor. Figure 3.7 illustrates the (4,8) connectivity of black points within

this Nano representation, further elucidating the spatial relationships and defining features of the image given in Figure 3.2.



Figure 3.7. (4,8) Connectivity and Nano Representation of the Image from Figure 3.2.

3.5. Image Segmentation

In the domain of image processing, image segmentation is a pivotal application central to most image-based operations. Image segmentation refers to the process of partitioning an image space into non-overlapping and meaningful homogeneous regions. While traditional image segmentation methods can face complications, especially when dealing with complex structures or poor image quality, rough set theory has proven to be a valuable methodology to overcome such challenges. Consequently, rough-set based image segmentation offers a stable and robust framework.

The segmentation of medical images, such as MRI brain scans, presents unique difficulties due to inherently poor image contrast, the presence of artifacts, and the often diffuse or missing boundaries of organs and tissues. The core principle behind segmentation utilizing rough sets is that, for a given set X (e.g., the tumor region), some cases (pixels) may be clearly labeled as belonging to X , while others are clearly labeled as not belonging to X . For an image universe U consisting of a collection of pixels, U can be partitioned into elementary units or arrays, where each array can be considered an indiscernible unit cell. In this proposed approach, the digital images are segmented specifically by leveraging the properties of Nano boundary approximations, which effectively define the precise outlines of the tumor. Figure 3.8 provides the resulting output of the digital image after this segmentation process.

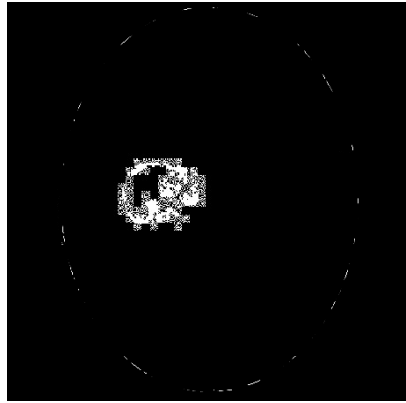


Figure 3.8

4. CONCLUSION

This paper introduces a novel application of Nano Digital Topology for the precise identification of brain tumors in digital MRI images. The proposed methodology systematically processes input MRI scans, beginning with essential preprocessing steps such as grayscale conversion, bias field correction, thresholding, and morphological thinning to prepare the image for analysis. The refined image is then transformed into a black and white grid, forming a formal digital picture upon which the core principles of Nano Digital Topology are applied.

By leveraging rough set theory, this approach effectively handles the inherent vagueness and uncertainty associated with medical image data, particularly in defining the ambiguous boundaries of brain tumors. The concepts of lower and upper approximations, along with the identification of Nano boundary points, provide a robust framework for delineating tumor regions that might be challenging for traditional methods. The final segmentation, derived from these nano approximations, aims to achieve precise, edge-to-edge detection, which is crucial for early and accurate diagnosis. This work demonstrates the potential of Nano Digital Topology to offer valuable insights into the structural characteristics of brain tumors, thereby potentially improving diagnostic accuracy and supporting clinical decision-making.

Future work will focus on implementing and validating these theoretical and practical results on larger, diverse datasets of brain tumor MRI images, exploring adaptive methods for parameter selection, and extending the application of Nano Digital Topology to other challenging medical image segmentation tasks.

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